

Lana Bergman Gašparić

Ispitivanje povezanosti hrapavosti površine cirkonij-oksidne keramike i vezne čvrstoće s obložnom keramikom: prethodno priopćenje

Correlation between Surface Roughness and Shear Bond Strength in Zirconia Veneering Ceramics: a Preliminary Report

Zavod za fiksnu protetiku Stomatološkog fakulteta Sveučilišta u Zagrebu
Department of Fixed Prosthodontics, School of Dental Medicine, University of Zagreb

Sažetak

Delaminacija i *chipping* obložne keramike opisani su kao najčešći uzroci za neuspjeh terapije cirkonij-oksidnim nadomjescima. **Svrha:** Željela se ustanoviti povezanost između hrapavosti površine jezgre od cirkonijeva oksida i vezne čvrstoće obložne keramike. **Materijali i postupci:** Sintetizirano je ukupno 10 uzoraka koji su bili podijeljeni u dvije skupine. Uzorci prve skupine polirani su, a oni iz druge polirani i pjeskareni. Nakon obrade površine cirkonij-oksidne jezgre napećena je obložna keramika debljine tri milimetra. Tako pripremljeni uzorci uloženi su u PTFE-kalupe s pomoću smole PMMA i izloženi sмиćnoj sili do pucanja (univerzalna kidalica). Hrapavost površine izmjerena je prije napećenja obložne keramike instrumentom s ticalom Pertherometer 58P, te su zabilježene vrijednosti Ra i Z. **Rezultati:** Polirani i pjeskareni uzorci imali su znatno hrapaviju površinu ($p<0,01$) te su pokazali mnogo više vrijednosti vezne čvrstoće ($p<0,01$) od samo poliranih uzoraka. **Zaključak:** Utvrđena je značajna povezanost između vrijednosti hrapavosti površine cirkonij-oksidne jezgre i vezne čvrstoće ($r=xy, p<0,01$) s obložnom keramikom.

Zaprimitljeno: 6. prosinca 2012.
Prihvatićen: 5. ožujka 2013.

Adresa za dopisivanje

Lana Bergman Gašparić
Sveučilište u Zagrebu Stomatološki fakultet
Zavod za fiksnu protetiku
Gundulićeva 5, 10 000 Zagreb
Tel: + 385 1 4802 111
Faks: + 385 1 4802 159
bergman@sfzg.hr

Ključne riječi

stomatološke ljske; cirkonij-oksid; keramika; svojstva površina; sмиćna sila; dentalni cementi;

Uvod

Krunice i mostovi višeslojni su objekti složene geometrije (1 – 3). Tradicionalno nastaju slojevanjem obložne keramike sloj po sloj na čvrsti jezgreni materijal (4,5). Strukturni integritet spoja između obložne keramike i jezgrenog materijala kritični je čimbenik koji utječe na trajnost potpuno keramičkog nadomjeska. Zato su delaminacija i *chipping* opisani kao najčešći uzroci neuspjeha u terapiji tim nadomjescima (6). Učestalost loma obložne keramike znatno je veća kod cirkonij-oksidne keramike u usporedbi s metal-keramičkim sustavima (7). Kvaliteta spoja između cirkonijeva oksida i obložne keramike do danas je nerazjašnjena. Veznu čvrstoću određuju mnogobrojni čimbenici – obrada površine jezgrenog materijala, snaga kemijskih veza, mehanička povezanost, vrsta i koncentracija defekata na međuspoju (8) te svojstvo vlaženja površine i stupanj naprezanja u sloju obložne keramike zbog razlike u koeficijentu termičke istezljivosti (KTI) jezgre i obložne keramike (9). U stomatologiji se najčešće rabi tritijem stabilizirani cirkonijev oksid (Y-TZP) visoke čvrstoće s koncentracijom kristalne faze većom od 90 posto (10).

Introduction

Dental crowns and bridges are generally laminar structures, with complex geometries (1-3). Traditionally, esthetic porcelain is veneered onto a strong core material layer by layer. In the case of all-ceramic restorations, the core material is usually zirconium (4, 5). The structural integrity of the interface between porcelain veneer and zirconia core is a critical factor in the longevity of all-ceramic dental crowns and fixed dental prostheses. That is why delamination and chipping of veneering porcelain were described as the most frequent reasons for the failure (6). The incidence of veneer fractures in zirconia FPDs was significantly higher compared to the metal-ceramic FPDs (7).

There is not much reliable information available about the bond quality between veneering ceramics and zirconia core. Bond strength is determined by many factors: surface finish of the core, strength of chemical bonds, mechanical interlocking, type and concentration of defects at the interface (8), wetting properties and the degree of compressive stress in the veneering layer due to difference in the coefficients of

Zato Y-TZP nije prikladan za jetkanje (11), pa se za obradu njegove površine primjenjuju druge metode kao, primjerice, pjeskarenje česticama aluminijeva oksida (12 – 15). Neka istraživanja pokazala su znatan utjecaj pjeskarenja i korištenja veznog sredstva na veznu čvrstoću (16 – 18). Tim načinima obrade smanjila se hrapavost površine i nastala su potkopana područja (19 – 22). No, pjeskarenje također inicira transformaciju zrna na površini te time utječe i na kvalitetu veze s obložnom keramikom (23,24). KTI monoklinskih zrna cirkonijeva oksida iznosi $7,5 \times 10^{-6}/^{\circ}\text{C}$, a KTI tetragonskih zrna je $10,8 \times 10^{-6}/^{\circ}\text{C}$. U skladu s tim povećanje razlike u KTI-u smanjuje veznu čvrstoću cirkonijeva oksida s obložnom keramikom (25). Zato je utjecaj pjeskarenja na mehanička svojstva Y-TZP-a, te na veznu čvrstoću s obložnom keramikom, još uvijek predmet mnogih istraživanja (23,26,27). Smični test uobičajeni je način mjerjenja vezne čvrstoće među slojevima kod potpuno keramičkih sustava (10,28 – 33).

Svrha istraživanja bila je ustanoviti povezanost između hrapavosti površine cirkonijeva oksida i vezne čvrstoće s obložnom keramikom.

Materijali i postupci

U istraživanju su korišteni blokovi presinteriranog cirkonijeva oksida IPS e.max ZirCAD (Ivoclar Vivadent AG, Schaan, Liechtenstein) podijeljeni u dvije skupine po pet uzoraka. Sinteriranjem u peći Programat S1 (Ivoclar Vivadent AG, Schaan, Liechtenstein) šest sati na temperaturi od 1500°C blokovi su dostigli dimenzije $10 \times 10 \times 10$ milimetara potrebne za istraživanje, pa glodanje nije bilo potrebno. Slijedilo je poliranje svih uzoraka dijamantnim svrdlima finoće $90 \mu\text{m}$ (Komet, Salzburg, Austrija) pod vodenim mlazom s maksimalnim brojem okretaja (200 000 rpm) i minimalnim pritiskom kako bi se osiguralo jednolično poliranje površine. Uzorci su očišćeni 70-postotnim etanolom, zatim deset sekundi vodenom parom te osušeni zrakom. Pet uzoraka podvrgnuto je mjerenu hrapavosti površine i na njih je napečena obložna keramika, a ostalih pet je naknadno pjeskareno (Renfert duo pro, GmbH, Hilzingen, Njemačka) česticama aluminijeva oksida ($110 \mu\text{m}$) (Cobra; Renfert, GmbH, Hilzingen, Njemačka) pod tlakom od 2,5 bara u trajanju od pet sekundi, očišćeno je parom, osušeno zrakom te ostavljeno za analizu površine i napečenje keramike.

Hrapavost površine izmjerena je instrumentom s ticalom Perthometer S8P (Perthen, Mahr, Göttingen, Njemačka). Pri mjerenu ticalo se kretalo po površini konstantnom brzinom i silom mjerjenja od $1,3 \text{ mN}$. Mjerena su obavljena Gaussovim filtrom s *cut-off* vrijednošću od $\lambda_c = 0,8 \text{ milimetara}$ i duljinom mjerjenja od $l_n = 5,6 \text{ milimetara}$. Srednja hrapavost (Ra) i Z-vrijednosti (udaljenost između najviše i najniže toč-

thermal expansion between zirconia and veneering ceramics (9). In contrast to conventional dental ceramics, the zirconia systems currently available for use in dentistry are high strength Y-TZP with a zirconium dioxide crystalline content higher than 90% (10). For this reason, Y-TZP ceramics are not suitable for acid etching (11), therefore, other surface treatment methods such as airborne particle abrasion with aluminum oxide particles (Al_2O_3) are used (11-15).

Some studies showed that the bonding strength and the mode of failure were significantly affected by surface treatments such as use of liners and sandblasting which increased the surface roughness and provided undercuts (16-22). However, sandblasting also initiates phase transition, thus affecting mechanical strength and most likely, the bonding capacity of the veneering material (23, 24). The coefficient of thermal expansion of monoclinic zirconia is $7.5 \times 10^{-6}/^{\circ}\text{C}$, and that of tetragonal zirconia is $10.8 \times 10^{-6}/^{\circ}\text{C}$. Accordingly, an increase in the difference in the coefficient of thermal expansion between the TZP framework and the veneering ceramic leads to a decrease in bond strength (25). Therefore, the effect of sandblasting on the mechanical strength of Y-TZP and the bond quality to veneering ceramics is an intensely discussed subject (23, 26, 27). To measure the bond strength of all-ceramic systems, shear tests are generally used to evaluate the influence of the core surface on bond quality (10, 28-33).

The aim of the study was to investigate the correlation between zirconia surface roughness and shear bond strength of veneering ceramics.

Materials and methods

Two groups of pre-sintered Y-TZP IPS e.max ZirCAD blocks (Ivoclar Vivadent AG, Schaan, Liechtenstein) were used in the study, each group consisting of 5 specimens. By sintering to full density in the Programat S1 furnace (Ivoclar Vivadent AG, Schaan, Liechtenstein) during 6 hours at the temperature of 1500°C , the blocks gained dimensions of $10 \times 10 \times 10 \text{ mm}$, so CAD/CAM grinding was not necessary. All samples were afterwards ground under water spray jet incorporated in the hand-piece with a $90 \mu\text{m}$ grit diamond bur (Komet, Salzburg, Austria) at the maximum revolutions (200,000 rpm) and with minimal pressure to ensure a consistent grinding speed. The cubes were cleaned with 70% ethanol, and then steam cleaned for 10 seconds and air dried. Five samples were left for surface roughness analysis and veneering, and other five samples were additionally sandblasted (Renfert duo pro, GmbH, Hilzingen, Germany) with $110 \mu\text{m}$ Al_2O_3 particles (Cobra; Renfert, GmbH, Hilzingen, Germany) at 2.5 bar pressure for a period of 5 seconds, steam-cleaned, air-dried and also left for surface roughness analysis and veneering.

The measurement of surface roughness was performed using the Stylus instrument Perthometer S8P (Perthen, Mahr, Göttingen, Germany). During the measurement the stylus moved at a constant speed across the samples with a measuring force of 1.3 mN . Measurements were performed by using Gauss filter with cut-off value of $\lambda_c = 0.8 \text{ mm}$ and the evaluation length $l_n = 5.6 \text{ mm}$. Mean roughness (Ra) and Z values (the distance from the highest to the lowest point of

ke na mjerenoj površini) zabilježene su za svaki uzorak te su statistički obrađene.

Na uzorce je tada tehnikom slojevanja napečena obložna keramika IPS e.max Ceram (Ivoclar Vivadent AG, Schaan, Liechtenstein). Kako bi se postigle odgovarajuće dimenzije obložne keramike (10 x 5 x 3 mm), bila su potrebna dva pečenja u peći Programat P700 (Ivoclar Vivadent AG, Schaan, Liechtenstein).

Test vezne čvrstoće proveden je univerzalnom kidalicom (model LXR, Lloyd Instruments, Fareham, Velika Britanija). Svaki je uzorak uložen u PTFE-kalupe s pomoću smole PMMA (Struers Co, Ballerup, Danska). Uzorci su postavljeni u kidaliku tako da je spoj dvaju materijala bio u razini njegina klina. Smična sila bila je usmjerena na spojnu površinu brzinom od jednog milimetra u minuti do loma koji se automatski bilježio računalom spojenim na kidaliku (Nexygen, Lloyd Instruments, Fareham, Velika Britanija).

Dobiveni podaci obrađeni su statističkim paketom SPSS (verzija 17.0, SPSS Inc., Chicago, IL, SAD). Nezavisnim t-testom ispitane su razlike među uzorcima. Piersonov koefficijent korelacije izračunat je između vrijednosti hrapavosti površine (R_a i Z) i vrijednosti vezne čvrstoće. P-vrijednosti manje od 0,05 smatraju se statistički značajnim.

Rezultati

Rezultati (tablice 1, 2 i 3) su pokazali značajan utjecaj hrapavosti površine na veznu čvrstoću s obložnom keramikom. Nakon smičnog testa analiza loma pokazala je da je obložna keramika napečena na drugu skupinu uzorka (polirani i pjeskareni) ostala vezana za površinu jezgrenog materijala pod znatno većim vrijednostima smične sile.

measurement along the observed line) were recorded for each sample and were statistically analysed.

Samples were then veneered using a layering technique. The used veneering ceramic was IPS e.max Ceram (Ivoclar Vivadent AG, Schaan, Liechtenstein). Two separate firings in a firing furnace Programat P700 under the same conditions were required to establish the correct dimensions of the veneering ceramics (10x5x3mm).

Each sample was then embedded in the customized polytetrafluoroethylene (PTFE) moulds using the PMMA resin AcryFix (Struers Co, Ballerup, Denmark) to allow shear bond testing in the universal testing machine (model LXR, Lloyd Instruments, Fareham, Great Britain), with the core-veneer interface positioned at the level of the jig. Shear force was applied as close as possible to the veneer-core interface at a crosshead speed of 1 mm/min until fracture occurred, which was automatically registered and displayed by the computer software of the testing machine (Nexygen, Lloyd Instruments, Fareham, Great Britain).

Statistical analysis was performed using SPSS statistical package (version 17.0, SPSS Inc., Chicago, IL, USA). Independent samples t-test was used to test the difference between samples. Pierson's coefficient of correlation was calculated between surface roughness values (Z and R_a value) and the shear bond strength values. P value of less than 0.05 was considered statistically significant.

Results

According to the results (Tables 1, 2 i 3), surface roughness showed significant influence on the bond strength of the veneering ceramics. After the shear bond strength test, the results of the fracture analysis showed that in the second group (ground and sandblasted samples) the veneering ceramic remained on the zirconia surface under significantly higher shear forces.

Tablica 1. Deskriptivna statistika i značajnost razlike vrijednosti vezne čvrstoće (N) između poliranih te poliranih i pjeskarenih uzorka
Table 1 Descriptive statistics and a significance of the difference for shear bond strength values (N) between ground, and ground and sandblasted samples

Obrada • ZrO_2 core treatment	N	X	SD	t	df	P
Vezna čvrstoća (N) • Shear bond strength (N)	Brušeni • Ground	5	264	55.5	- 5.89	<0.01
	Brušeni i pjeskareni • Ground and sandblasted	5	450	44.1		

N = broj uzorka • number of samples; x = srednje vrijednosti • mean values; SD = standardna devijacija • standard deviation; t = t vrijednost • t value; df = stupanj slobode • degree of freedom; p = p vrijednost • p value

Tablica 2. Deskriptivna statistika i značajnost razlike Z- i R_a -vrijednosti (μm) hrapavosti površine između samo poliranih te poliranih i pjeskarenih uzorka
Table 2 Descriptive statistics and a significance of the difference for surface roughness values (Z values) (μm) and R_a values (mean roughness) (μm) between ground and ground and sandblasted samples

Obrada • ZrO_2 core treatment	N	X	SD	t	df	P
Z vrijednost (μm) • Z value (μm)	Brušeni • Ground	5	4.03	0.16	- 8.84	<0.01
	Brušeni i pjeskareni • Ground and sandblasted	5	5.48	0.33		
Srednja hrapavost (R_a) (μm) • Mean roughness (R_a) (μm)	Brušeni • Ground	5	0.77	0.04	- 4.69	<0.01
	Brušeni i pjeskareni • Ground and sandblasted	5	0.95	0.07		

N = broj uzorka • number of samples; x = srednje vrijednosti • mean values; SD = standardna devijacija • standard deviation; t = t vrijednost • t value; df = stupanj slobode • degree of freedom; p = p vrijednost • p value

Tablica 3. Korelacija između vezne čvrstoće (N) i vrijednosti hrapavosti površine (μm)
Table 3 Correlation between shear bond strength (N) and surface roughness values (μm)

	Z vrijednost • Z value (μm)	Srednja hrapavost • Mean roughness (Ra) (μm)
Vezna čvrstoća (N) • Shear bond strength (N)	Pearsonova korelacija • Pearson Correlation	0.88**
	P (2-tailed)	<0.01
	N	10

** Correlation is significant at the 0.01 level (2-tailed)

Rasprava

Protetski nadomjestak pacijenti bi trebali u cijelosti prihvatići jer im na dulje razdoblje nadoknađuje funkciju i estetiku (34 – 36). Cirkonij-oksidna keramika danas je jedan od najčešće korištenih sustava potpune keramike, kako za sanaciju pojedinačnim krunicama tako i u mosnim konstrukcijama. U kliničkom radu uočilo se da nastaju gubici funkcijске trajnosti nadomjestka zbog dvaju problema – delaminacije i *chippinga* dijela obložne keramike. Kako bi se otkrio uzrok (8, 9) i pokušao eliminirati taj problem, površina cirkonij-oksidne jezgre tretirala se na različite načine (19 – 23). Pjeskarenje je jedan od mogućih načina obrade kako bi se postigla snažna veza s obložnom keramikom. No, naprezanje izazvano tim postupkom inicira transformaciju zrna cirkonijeva oksida na površini u monoklinsku fazu koja je volumenom veća te rezultira tlačnim naprezanjem i smanjenjem koeficijenta termičke istezljivosti (23, 24, 37, 38). Iz tog razloga transformirana se zrna trebaju vratiti u tetragonalnu fazu postupkom koji se naziva regeneracijsko pečenje, čime se usklađuje KTI (24).

Vezna čvrstoća je ključno naprezanje koje materijal može podnijeti do loma kad ga se izloži smičnom opterećenju. Osobito je važna kod svih istraživanja koja proučavaju spojeve dvaju materijala kod višeslojnih sustava (39).

U ovom istraživanju procjenjivale su se promjene morfologije i hrapavosti površine cirkonijeva oksida. Pjeskarenje česticama aluminijskog oksida veličine 50 i 125 μm provedeno je referirajući se na prijašnje studije (22, 25, 26, 40). Nakamura i suradnici (41) zabilježili su povećanje vezne čvrstoće između Y-TZP-a i obložne keramike zahvaljujući povećanju hrapavosti površine uzrokovano pjeskarenjem. No, druga studija pokazala je smanjenje vezne čvrstoće pjeskarenjem (42). Iako neke studije upućuju na to da se vezna čvrstoća povećava povećanjem hrapavosti površine, u drugima se, pak, ističe da transformacija zrna na površini utječe na smanjenje vezne čvrstoće (25). Kad je riječ o problemu vezne čvrstoće, još se vode mnogobrojne polemike, pa se ovim istraživanjem željela ustavoviti povezanost hrapavosti površine i vezne čvrstoće obložne keramike. Dokazano je da hrapavost površine značajno utječe na veznu čvrstoću. Nakon testa vezne čvrstoće, rezultati analize loma pokazali su da je u drugoj skupini uzoraka (polirani i pjeskareni) obložna keramika ostala na površini cirkonijeva oksida nakon znatno većih smičnih sila. Može se zaključiti da je adhezivna čvrstoća obložne keramike veća od kohezivne. Najslabija karika nije spoj cirkonijeva oksida i obložne keramike, nego sama obložna keramika. Pjeskarenje je nahrapavilo, te time pove-

Discussion

Prosthetic appliance must be fully accepted by the patient to increase his/her quality of life, but it also has to show long term durability and clinical quality (34-36). Zirconia is one of the most frequently used all-ceramic systems for dental crowns and FPDs. However, during clinical use, it has been observed that delamination and chipping were the most frequent reasons for failure. To discover the cause of failure (8, 9), the surface of zirconia core has been variously pre-treated (19-23). Air-abrasion of the zirconia surface is an important treatment method in achieving strong bond to veneering porcelain. However, the mechanical stress initiates a phase transition to monoclinic zirconia, and the phase transition gives rise to volume expansion resulting in compressive stress and reduction in coefficient of thermal expansion (23, 24, 37, 38). Therefore, the phase transition needs to be reversed to the tetragonal zirconia by recommended heat treatment prior to veneering also known as regeneration firing, with a concomitant alteration in the coefficient of thermal expansion (24).

Shear strength is the maximum stress that a material can withstand before failure in a shear mode of loading and is particularly valuable in the study of interfaces between materials (39). This study evaluated the surface morphology and roughness of Y-TZP ceramic material after grinding as well as grinding and sandblasting in relation to shear bond strength of the bi-layered veneering ceramics. Sandblasting with 50 and 125 μm alumina was performed with reference to earlier studies (22, 25, 26, 40). Nakamura et al. (41) reported that bond strength between TZP and veneering ceramics increased due to a rise in the surface roughness of the TZP by sandblasting. However, another study reported that bond strength decreased (42). Although some studies have indicated that bond strength increases on surfaces with increased roughness, others have suggested that phase transformation of TZP by sandblasting may adversely affect bond strength (25). There is still a lot of controversy concerning this problem, so we aimed to find a correlation between surface roughness of zirconia samples and shear bond strength values of veneered ceramics. In the present study, surface roughness showed significant influence on the bond strength. After the shear test, the results of the fracture analysis showed that in the second group (ground and sandblasted samples) the veneering ceramic remained on the zirconia surface under significantly higher shear forces. It could be concluded that the adhesive strength between zirconia and the veneering ceramic was higher than the cohesive strength of the veneering ceram-

čalo i preoblikovalo, veznu površinu cirkonij-oksidne keramike. Kim i suradnici proveli su *in vitro* studiju čiji su rezultati pokazali da pjeskarenje znatno povećava veznu čvrstoću s obložnom keramikom, za razliku od aplikacije veznog sredstva (32). No, rezultati Fischera i njegovih kolega pokazuju da se pjeskarenje i regeneracijsko pečenje ne preporučuju kao načini obrade površine (4).

Rezultati dobiveni u ovom istraživanju upućuju na snažnu i značajnu povezanost parametara hraptavosti površine i vrijednosti vezne čvrstoće te se ističu potreba za dalnjim istraživanjima na većem broju uzoraka.

Zaključak

Ustanovljena je međusobna povezanost hraptavosti površine cirkonijeva oksida i vezne čvrstoće s obložnom keramikom te će se daljnja istraživanja usmjeriti prema rasyjetljavanju problema povezanosti navedenih parametara na većem broju uzoraka.

Zahvala

Istraživanje je provedeno u sklopu projekta 065-0650446-0435 odobrenog u Ministarstvu znanosti i obrazovanja Republike Hrvatske.

Sukob interesa

Nije bilo sukoba interesa.

Abstract

Delamination and chipping of veneering porcelain were described as the most frequent reasons for the failure of zirconia fixed partial dentures. **Aim:** The aim of the study was to assess the correlation of surface roughness and the shear bond strength of veneering ceramics to zirconia core. **Materials and methods:** A total number of 10 zirconia samples, 5 in each group were sintered. Samples in the first group were ground, and in the second were ground and sandblasted. After the surface treatment, veneering ceramic was fired to the core up to the thickness of 3 mm, the samples were embedded in the PTFE molds using PMMA resin and subjected to shear force until fracture occurred. The surface roughness was assessed prior to application of veneering ceramics by the Stylus instrument Perthometer S8P and Ra (mean roughness) and Z values (distance from the highest to the lowest point of measurement along the observed line) were obtained. **Results:** Ground and sandblasted samples had significantly rougher surface ($p<0.01$) and showed significantly higher shear bond strength ($p<0.01$). **Conclusion:** The positive and significant correlation was found between surface roughness values and shear bond strength. Further research is needed to completely elucidate the observed relation.

Received: December 6, 2012

Accepted: March 5, 2013

Address for correspondence

Lana Bergman Gašparić
University of Zagreb, School of Dental Medicine
Department of Fixed Prosthodontics
Gundulićeva 5, 10 000 Zagreb
Tel: + 385 1 4802 111
Fax: + 385 1 4802 159
bergman@sfzg.hr

Key words

Dental Veneers; Zirconium oxide;
Ceramics; Surface Properties; Shear Strength; Dental Cements

References

1. Kelly JR. Dental ceramics: current thinking and trends. Dent Clin North Am. 2004 Apr;48(2):viii, 513-30.
2. Denry I, Kelly JR. State of the art of zirconia for dental applications. Dent Mater. 2008 Mar;24(3):299-307.
3. Dautović-Kazazaić L, Redžepagić S, Ajanović M, Gavranović A, Strujić S. Periodontal evaluation of patients with ceramic fused-to-metal and acrylate fused-to-metal crowns over a period of 1-5 years. Acta Stomatol Croat. 2010;44(1):34-46.
4. Kelly JR. Clinically relevant approach to failure testing of all-ceramic restorations. J Prosthet Dent. 1999 Jun;81(6):652-61.
5. Deng Y, Miranda P, Pajares A, Guiberteau F, Lawn BR. Fracture of ceramic/ceramic/polymer trilayers for biomechanical applications. J Biomed Mater Res A. 2003 Dec 1;67(3):828-33.
6. Saied MA, Lloyd IK, Haller WK, Lawn BR. Joining dental ceramic layers with glass. Dent Mater. 2011 Oct;27(10):1011-6.
7. Sailer I, Pjetursson BE, Zwahlen M, Hämmерle CH. A systematic review of the survival and complication rates of all-ceramic and metal-ceramic reconstructions after an observation period of at least 3 years. Part II: Fixed dental prostheses. Clin Oral Implants Res. 2007 Jun;18 Suppl 3:86-96.

8. Mehulić K, Svetlicić V, Segota S, Vojvodić D, Kovacić I, Katanec D et al. A study of the surface topography and roughness of glazed and unglazed feldspathic ceramics. *Coll Antropol.* 2010 Mar;34 Suppl 1:235-8.
9. Isgrò G, Pallav P, van der Zel JM, Feilzer AJ. The influence of the veneering porcelain and different surface treatments on the bi-axial flexural strength of a heat-pressed ceramic. *J Prosthet Dent.* 2003 Nov;90(5):465-73.
10. Fischer J, Grohmann P, Stawarczyk B. Effect of zirconia surface treatments on the shear strength of zirconia/veneering ceramic composites. *Dent Mater J.* 2008 May;27(3):448-54.
11. Luthardt RG, Holzhüter M, Sandkuhl O, Herold V, Schnapp JD, Kuhlisch E et al. Reliability and properties of ground Y-TZP-zirconia ceramics. *J Dent Res.* 2002 Jul;81(7):487-91.
12. Kern M, Wegner SM. Bonding to zirconia ceramic: adhesion methods and their durability. *Dent Mater.* 1998 Jan;14(1):64-71.
13. Senyilmaz DP, Palin WM, Shortall AC, Burke FJ. The effect of surface preparation and luting agent on bond strength to a zirconium-based ceramic. *Oper Dent.* 2007 Nov-Dec;32(6):623-30.
14. Della Bona A, Borba M, Benetti P, Cecchetti D. Effect of surface treatments on the bond strength of a zirconia-reinforced ceramic to composite resin. *Braz Oral Res.* 2007 Jan-Mar;21(1):10-5.
15. Oyagüe RC, Monticelli F, Toledano M, Osorio E, Ferrari M, Osorio R. Effect of water aging on microtensile bond strength of dual-cured resin cements to pre-treated sintered zirconium-oxide ceramics. *Dent Mater.* 2009 Mar;25(3):392-9.
16. de Oyagüe RC, Monticelli F, Toledano M, Osorio E, Ferrari M, Osorio R. Influence of surface treatments and resin cement selection on bonding to densely-sintered zirconium-oxide ceramic. *Dent Mater.* 2009 Feb;25(2):172-9.
17. Uo M, Sjögren G, Sundh A, Goto M, Watari F, Bergman M. Effect of surface condition of dental zirconia ceramic (Denzir) on bonding. *Dent Mater J.* 2006 Sep;25(3):626-31.
18. Kim HJ, Lim HP, Park YJ, Vang MS. Effect of zirconia surface treatments on the shear bond strength of veneering ceramic. *J Prosthet Dent.* 2011 May;105(5):315-22.
19. Saito A, Komine F, Blatz MB, Matsumura H. A comparison of bond strength of layered veneering porcelains to zirconia and metal. *J Prosthet Dent.* 2010 Oct;104(4):247-57.
20. Luthardt RG, Sandkuhl O, Reitz B. Zirconia-TZP and alumina--advanced technologies for the manufacturing of single crowns. *Eur J Prosthodont Restor Dent.* 1999 Dec;7(4):113-9.
21. Aboushelib MN, de Jager N, Kleverlaan CJ, Feilzer AJ. Microtensile bond strength of different components of core veneered all-ceramic restorations. *Dent Mater.* 2005 Oct;21(10):984-91.
22. Aboushelib MN, Kleverlaan CJ, Feilzer AJ. Microtensile bond strength of different components of core veneered all-ceramic restorations. Part II: Zirconia veneering ceramics. *Dent Mater.* 2006 Sep;22(9):857-63.
23. Kosmac T, Oblak C, Jevnikar P, Funduk N, Marion L. The effect of surface grinding and sandblasting on flexural strength and reliability of Y-TZP zirconia ceramic. *Dent Mater.* 1999 Nov;15(6):426-33.
24. Guazzato M, Quach L, Albakry M, Swain MV. Influence of surface and heat treatments on the flexural strength of Y-TZP dental ceramic. *J Dent.* 2005 Jan;33(1):9-18.
25. Paliska J, Stipetić A, Tarle Z, Ristić M, Ban T, Vujičić N, Pichler G. Colorimetric assessment of different whitening procedures. *Acta Stomatol Croat.* 2011;45(4):258-67.
26. Kosmac T, Oblak C, Jevnikar P, Funduk N, Marion L. Strength and reliability of surface treated Y-TZP dental ceramics. *J Biomed Mater Res.* 2000;53(4):304-13.
27. Zhang Y, Lawn BR, Malament KA, Van Thompson P, Rekow ED. Damage accumulation and fatigue life of particle-abraded ceramics. *Int J Prosthodont.* 2006 Sep-Oct;19(5):442-8.
28. Al-Dohan HM, Yaman P, Dennison JB, Razzoog ME, Lang BR. Shear strength of core-veneer interface in bi-layered ceramics. *J Prosthet Dent.* 2004 Apr;91(4):349-55.
29. Dündar M, Ozcan M, Cömlekoglu E, Güngör MA, Artunç C. Bond strengths of veneering ceramics to reinforced ceramic core materials. *Int J Prosthodont.* 2005 Jan-Feb;18(1):71-2.
30. Dündar M, Ozcan M, Gökcé B, Cömlekoglu E, Leite F, Valandro LF. Comparison of two bond strength testing methodologies for bi-layered all-ceramics. *Dent Mater.* 2007 May;23(5):630-6.
31. Mosharraf R, Rismanchian M, Savabi O, Ashtiani AH. Influence of surface modification techniques on shear bond strength between different zirconia cores and veneering ceramics. *J Adv Prosthodont.* 2011 Dec;3(4):221-8.
32. Kim HJ, Lim HP, Park YJ, Vang MS. Effect of zirconia surface treatments on the shear bond strength of veneering ceramic. *J Prosthet Dent.* 2011 May;105(5):315-22.
33. Choi BK, Han JS, Yang JH, Lee JB, Kim SH. Shear bond strength of veneering porcelain to zirconia and metal cores. *J Adv Prosthodont.* 2009 Nov;1(3):129-35.
34. Gasparić LB, Catović A, Komar D, Bergman V, Catić A. Epidemiological study on prosthodontic appliance deliveries within elderly cohorts in the Republic of Croatia, 2002-2006. *Coll Antropol.* 2009 Jun;33(2):461-5.
35. Umer F, Raza Khan F, Khan A. Golden proportion in visual dental smile in Pakistani population: a pilot study. *Acta Stomatol Croat.* 2010;44(3):168-175.
36. Ortolan SM, Viskić J, Stefancić S, Sitar KR, Vojvodić D, Mehulić K. Oral hygiene and gingival health in patients with fixed prosthodontic appliances-a 12-month follow-up. *Coll Antropol.* 2012 Mar;36(1):213-20.
37. Deville S, Chevalier J, Gremillard L. Influence of surface finish and residual stresses on the ageing sensitivity of biomedical grade zirconia. *Biomaterials.* 2006 Apr;27(10):2186-92.
38. Sato H, Yamada K, Pezzotti G, Nawa M, Ban S. Mechanical properties of dental zirconia ceramics changed with sandblasting and heat treatment. *Dent Mater J.* 2008 May;27(3):408-14.
39. Powers JM, Sakaguchi RL. Craig's restorative dental materials. St. Louis: Mosby; 2006.
40. Aboushelib MN, Kleverlaan CJ, Feilzer AJ. Effect of zirconia type on its bond strength with different veneer ceramics. *J Prosthodont.* 2008 Jul;17(5):401-8.
41. Nakamura T, Wakabayashi K, Zaima C, Nishida H, Kinuta S, Yatani H. Tensile bond strength between tooth-colored porcelain and sandblasted zirconia framework. *J Prosthodont Res.* 2009 Jul;53(3):116-9.
42. Kim ST, Cho HJ, Lee YK, Choi SH, Moon HS. Bond strength of Y-TZP-zirconia ceramics subjected various surface roughening methods and layering porcelain. *Surf Interface Anal.* 2010;42(6-7):576-80.